

1 **On-chip diamond MEMS magnetic sensing through multifunctionalizing**
2 **magnetostrictive thin film**

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11

12 **Abstract**

13 Electrically integrable, high-sensitivity, and high-reliability magnetic sensors have not yet
14 been realized at high temperatures (500 °C). In this study, we demonstrate an integrated on-
15 chip single-crystal diamond (SCD) micro-electromechanical system (MEMS) magnetic
16 transducer by coupling SCD with a large magnetostrictive FeGa film. The FeGa film is
17 multifunctionalized to actuate the resonator, self-sense the external magnetic field, and
18 electrically read the resonance signal. The on-chip SCD MEMS transducer shows a high-
19 sensitivity of 3.2 Hz/mT from room temperature to 500 °C and a low noise level of 9.45
20 nT/Hz^{1/2} up to 300 °C. The minimum fluctuation of the resonance frequency is 1.9×10^{-6} at
21 room temperature and 2.3×10^{-6} at 300 °C. An SCD MEMS resonator array with parallel
22 electric readout is subsequently achieved, thus providing a basis for the development of
23 magnetic image sensors. The present study facilitates the development of highly integrated on-
24 chip MEMS resonator transducers with high performance and high thermal stability.

25

26 **Keywords:** Single-crystal diamond, MEMS, on-chip actuation and sensing, magnetic sensor

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30 1. Introduction

31 Real-time health care of human beings for Internet of Things, precise biomedical diagnosis,
32 and infrastructure maintenance, particularly under extreme conditions, increases the immediate
33 demand for developing integrated magnetic sensing technology with high sensitivity, high
34 reliability, low power consumption, and minimized size.^[1-8] The current magnetic sensors
35 primarily include superconducting quantum interference device (SQUID) sensors, Hall sensors,
36 fluxgate sensors, magneto-resistive (MR) sensors, nitrogen-vacancy (NV) sensors, and micro-
37 electromechanical system (MEMS) sensors.^[2, 9-14] The SQUID sensors with the highest
38 magnetic resolution of fT level require high cost and liquid nitrogen/helium as a refrigerant,
39 which render them less advantageous compared with other magnetic sensors.^[15] For Hall
40 sensors, their low sensitivity and resolution limit their performance and applications.^[14]
41 Fluxgate sensors require complex processes to fabricate their magnetic cores and coils, which
42 feature large masses and high power consumption.^[16] The restricted magnetic field magnitude
43 appearance of MR sensors suppresses their application regimes.^[17] Another promising magnetic
44 sensor is based on the NV center in diamond, which in principle shows high sensitivity and
45 nanoscale resolution. However, the controllability of the NV center and the electrical readout
46 of NV signals are challenging.^[18-20] MEMS technology exhibits the merits of batch fabrication,
47 controllability in dimensions down to the nanoscale, low power consumption, low cost, high
48 sensitivity, and high integration.^[21]

49 In addition, for harsh application fields such as mineral/oil exploration, space exploration,
50 high-temperature magnetic valves, and engine and transmission speed control in cars, magnetic
51 sensors with high thermal-stability performance are in high demand.^[22, 23] Recently, the main
52 high-temperature magnetic sensors, including MR sensors, fluxgate sensors, and Hall sensors,
53 are affected by material and physical limitations under extreme conditions, which result in low
54 sensitivity, weak thermal stability, and restrained operating temperatures.^[24-26] MEMS
55 resonators coupled with soft magnetic materials provide a new paradigm for fabricating various

56 magnetic transducers.^[27, 28] Furthermore, a MEMS resonator array with high integration can be
57 developed, which yields efficient and precise special mapping of magnetic fields.^[29] To develop
58 MEMS magnetic sensor arrays, all electrical actuation and sensing are necessary for integration
59 with electronics.

60 Single-crystal diamond (SCD) is a promising material for high-performance and high-
61 reliability MEMS devices owing to its outstanding physical, chemical, mechanical, and
62 electrical properties.^[30-42] SCD MEMS resonators combined with galferol (FeGa), a material
63 with a large magnetostrictive coefficient of 375 ppm and an ultrahigh Curie temperature of
64 675 °C, provide an ideal scheme for high-sensitivity and thermal-stability magnetic transducers
65 *via* the delta-E (ΔE) effect.^[43, 44] To achieve highly integrated high-sensitivity SCD MEMS
66 transducers, all-electrical on-chip actuation and sensing are required.^[45] The piezoelectric effect
67 and electrostatic or dielectric actuation with capacitive sensing were developed to fulfill the
68 functions of actuation and readout.^[46-49] The piezoelectric method offers an efficient route with
69 high electromechanical coupling efficiency, but the energy dissipation induced by the
70 multilayer degrades the sensitivity. The dielectric actuation overcomes the energy dissipation
71 problem, and an off-chip bulky optical readout was achieved.^[50] For highly integrated MEMS
72 magnetic sensors, a scheme with multiple functions including actuation, sensing, and signal
73 readout is desired. In this study, we propose and demonstrate an on-chip SCD MEMS magnetic
74 sensor by multifunctionalizing a magneto-strictive FeGa film for harmonic actuation, magnetic
75 sensing, and resonance signal readout. To enhance adhesion at the interface between FeGa and
76 the SCD, a Ti thin film was added to form a FeGa/Ti/SCD magnetic transducer. The magnetic
77 transducer fulfilled magnetic transducing performance with high-temperature operation up to
78 500 °C, a sensitivity of 3.2 Hz/mT from room temperature to 500 °C, and a low noise level of
79 9.45 nT/Hz^{1/2} at 300 °C. The fluctuation of the resonance frequency was 1.9×10^{-6} at room
80 temperature and 2.3×10^{-6} at 300 °C. Furthermore, a prototype magnetic transducer array based
81 on on-chip FeGa/Ti/SCD MEMS magnetic transducers was developed. This study provides a

82 promising strategy for developing highly integrated MEMS magnetic transducers with high
83 performance and reliability, which are superior to the present magnetic transducers.

84 **2. Results and Discussion**

85 SCD cantilevers with an SCD-on-SCD structure provide a robust platform for fabricating
86 MEMS magnetic transducers. The fabrication process of the SCD cantilever-based magnetic
87 transducer is shown in **Figure S1 (Supporting Information)**. First, bare SCD cantilevers were
88 fabricated via the smart-cut technique, which primarily includes carbon ion implantation,
89 diamond growth, photolithography treatment, metal mask deposition, reactive ion etching, and
90 structure release. The bare SCD cantilevers fabricated via this technique exhibit high reliability
91 and high Q factors. The details of this approach for batch production are available in our
92 previous publication.^[51, 52] Subsequently, a 2-nm-thick Ti film followed by a 90-nm-thick FeGa
93 film was deposited on the bare SCD cantilevers using a magnetron sputtering system, followed
94 by a 1-nm-thick Ti film and a 7-nm-thick Au film using an e-beam evaporator system. The 90
95 nm FeGa thin film is a trade-off for the quality (Q) factor of the SCD resonator and the
96 optimization of the magnetic properties of the FeGa thin film. The thick FeGa film resulted in
97 a reduced Q factor, whereas the thin FeGa film degraded the magnetic properties.

98 **2.1 Resonator elasticity vibration theory**

99 The mechanical vibration characteristics of a rectangular uniform cantilever beam can be
100 described and analyzed based on the Euler–Bernoulli law (see the SI).^[53] The resonance
101 frequency of the fundamental (first) mode is expressed as

$$102 \quad f = 0.162 \frac{t_{th}}{L^2} \sqrt{\frac{E}{\rho}}, \quad (1)$$

103 where E and ρ are the Young's modulus and mass density of the beam, respectively; and L and
104 t_{th} denote beam length and thickness, respectively. The resonance frequency is determined by
105 the dimensions and material properties of the cantilever.

106 **2.2 Self-sensing and actuation of cantilever resonance**

107 In this study, Au/FeGa/Ti was deposited on the SCD substrate as the gate (G) electrode
 108 for on-chip actuation and on the SCD cantilevers as source–drain (S–D) electrodes to sense the
 109 magnetic fields and electrically readout the resonance signal. **Figure 1a** shows the actuation
 110 and readout circuits of the on-chip SCD resonator. The ultimate optical feature of a 160- μm -
 111 long SCD cantilever magnetic transducer is shown in **Figure 1b**. A radio-frequency (RF) signal
 112 with an amplitude of V_g^{ac} and a frequency of ω was applied to the G electrode. Another RF signal
 113 with an amplitude of V_{sd}^{ac} and a frequency of $\omega + \Delta\omega$ was connected to the S–D electrodes to read
 114 out the vibration signal. For a certain gate voltage V_g , a charge q was induced on the cantilever,
 115 which is expressed as $q = C_g V_g$, where C_g is the capacitance between the G electrode and
 116 cantilever. The electrostatic force results in the bending of the cantilever. In this study, $V_g = V$
 117 $^{ac} \cos(\omega\tau)$. The total energy stored in the capacitor is $E_{eng} = 1/2 C_g(z) V_g^2$,^[54] where z is the distance
 118 between the G electrode and cantilever. The total electrostatic force on the cantilever is
 119 expressed as^[54]

$$120 \quad F_{el} = \frac{\partial E_{eng}}{\partial z} = \frac{1}{2} \frac{dC_g}{dz} (V_g^{ac} \cos \omega\tau)^2 \quad (2)$$

121 $V_g^{ac} \cos(\omega\tau)$ results in a periodic electric force that causes the cantilever to vibrate. The
 122 displacement of the cantilever is the largest when the driving frequency is at its resonance
 123 frequency.

124 The signal readout resulting from the cantilever motion is based on the piezoresistive effect
 125 of the S–D electrode on the cantilever. To characterize the output signal, a modulation
 126 frequency $\Delta\omega$ of 5 kHz was set. The output signal generated at the S electrode is a mixture of
 127 signals from the G and D electrodes, which is expressed as^[55, 56]

$$128 \quad V_{out} = \frac{\Delta R_0}{R + R_0} V_{sd}^{ac} [\cos(\Delta\omega\tau - \varphi) + \cos((2\omega + \Delta\omega)\tau + \varphi)], \quad (3)$$

129 where R is the circuit resistance; R_0 is the resistance of the electrode deposited on the cantilever,
 130 which is approximately 100 Ω ; V_{sd}^{ac} is the voltage applied to the S–D electrodes; and ΔR_0
 131 represents the resistance change of the metal electrode on the cantilever owing to its vibration

132 motion. The bias signal mixes with the vibration motion of the metal electrode and generates
 133 signals at frequencies $\Delta\omega$ and $2\omega+\Delta\omega$. A low-pass filter was utilized to filter the frequency of
 134 $2\omega+\Delta\omega$. The remaining signals were fed into a lock-in amplifier for the readout. The output
 135 signal at a frequency of $\Delta\omega$ is expressed as

$$136 \quad V_{out} = \frac{\Delta R_0}{R+R_0} V_{sd}^{ac} \cos(\Delta\omega\tau - \varphi) \quad (4)$$

137 The amplitude of the output voltage reached its maximum value when the cantilever vibrated
 138 at its resonance frequency. Thus, the SCD cantilever with the actuation and sensing structure
 139 can realize the actuation and detection of mechanical motion. This actuation and sensing
 140 scheme provides a strategy to design MEMS devices with an electrical interface for integration
 141 with electronics.

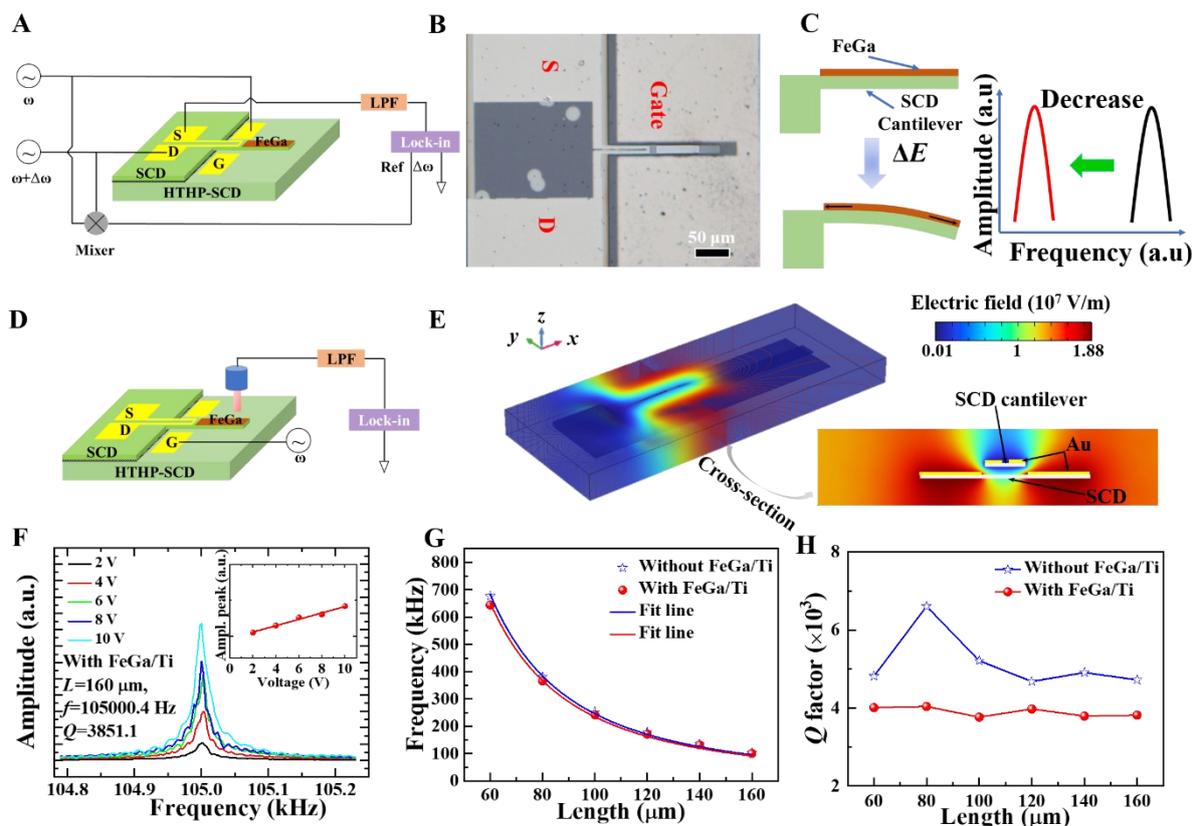
142 *2.3 Magnetic sensing principle based on ΔE effect*

143 For a magnetostrictive material, the Young's modulus changes during the magnetization
 144 process, which is known as the ΔE effect.^[57, 58] The ΔE effect is expressed as

$$145 \quad \Delta E = E_0 - E_H, \quad (5)$$

146 where E_0 and E_H are Young's moduli of the material without and with the application of a
 147 magnetic field, respectively. The ΔE effect of the ferromagnetic thin film deposited on the SCD
 148 cantilever is regarded as the magnetic sensing principle. **Figure 1c** schematically shows the
 149 fundamental sensing principle of the magnetic transducer based on the SCD cantilever structure.
 150 By applying an external magnetic field, the SCD cantilever is subjected to bending stress
 151 induced by the FeGa film. The shape of the FeGa film varies depending on the ΔE effect, which
 152 results in a change in its Young's modulus. Consequently, the effective Young's modulus of
 153 the SCD-based cantilever with multiple layers changes. Subsequently, the resonance frequency
 154 of the SCD-based cantilever shifts owing to the ΔE effect. The magnetic sensitivity of the SCD-
 155 based cantilever transducer is characterized as the resonance frequency response to the
 156 magnetic field.

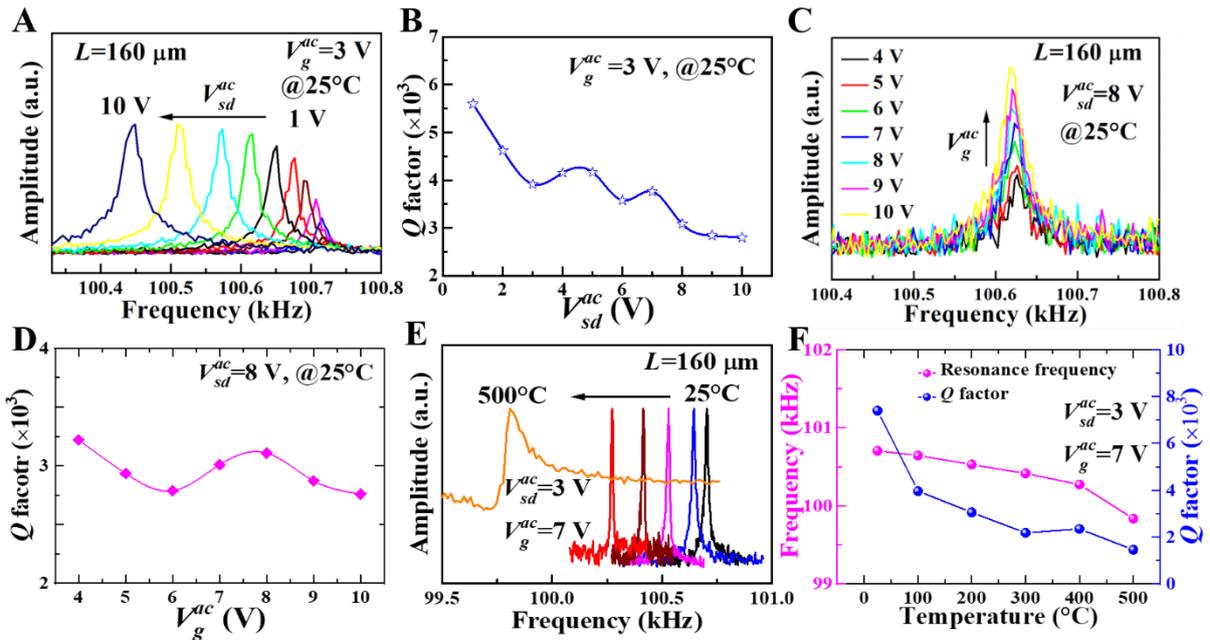
157 2.4 Fundamental mechanical resonance



158
 159 **Figure 1.** Measurement setup and resonance performances of the SCD-based resonators. A)
 160 Schematic diagram of the measurement setup for the SCD-based cantilever magnetic transducer
 161 with the on-chip self-sensing and actuation configuration. LPF: low frequency filter. B) Optical
 162 images of a 160- μm -long SCD-based cantilever magnetic transducer. C) Magnetic sensing
 163 principle of a cantilever resonator with resonance frequency shift. D) Schematic image of the
 164 measurement setup with an optical readout system. E) Simulation of the electric field
 165 distribution of a SCD-based resonator with on-chip actuation. S–D electrodes are grounded and
 166 $V_g^{ac} = 1$ V. F) Typical resonance frequency spectra of a 160- μm -long SCD-based cantilever.
 167 Inset shows the motion amplitude with linear dependence on the gate voltage. G) Resonance
 168 frequencies and H) Q factors of SCD-based cantilevers dependence on length L without and
 169 with deposition of FeGa/Ti film.

170
 171 To investigate the harmonic oscillation characteristics of SCD-based cantilevers, the S–D
 172 electrodes were grounded and the G electrode was connected to an RF signal source. A laser
 173 Doppler vibrometer was utilized to analyze the harmonic signal of the SCD-based oscillator, as
 174 shown in **Figure 1d**.^[51, 52] The electric field distribution of the SCD-based oscillator was

175 simulated using the COMSOL software as the S–D electrodes were grounded and $V_g^{ac} = 1$ V,
 176 which reflected the electric field confined around the SCD cantilever (**Figure 1e and Figure**
 177 **S2, Supporting Information**) The gate voltage did not significantly affect the resonance
 178 frequency (**Figure 1f**) and linearly enhanced the amplitude of the resonance spectrum (the inset
 179 of **Figure 1f**). The dependence of the resonance frequency on the length of the oscillator with
 180 and without the deposition of FeGa/Ti films is depicted in **Figure 1g**. The dependences of the
 181 resonance frequency of the SCD-based oscillator with and without FeGa/Ti films on the length
 182 agreed well with **Equation 1**. The Q factors of the SCD oscillators decrease after the deposition
 183 of the FeGa/Ti films (**Figure 1h and Equation S6, Supporting Information**) but remained as
 184 high as approximately 4000.



185
 186 **Figure 2.** Resonance performances of the SCD-based cantilever transducer with on-chip
 187 actuation and sensing scheme. A) Resonance frequency spectra of a 160- μm -long SCD-based
 188 cantilever transducer measured by the electrical readout system at various V_{sd}^{ac} and $V_g^{ac} = 3$ V
 189 @25 °C. The resonance frequency shifts downward as V_{sd}^{ac} increases. B) Dependences of Q
 190 factors on V_{sd}^{ac} at $V_g^{ac} = 3$ V @25 °C. C) Resonance frequency spectra of a 160- μm -long SCD-
 191 based cantilever transducer measured by the electrical readout system at various V_g^{ac} and $V_{sd}^{ac} =$
 192 8 V @25 °C. D) Variations in Q factors with V_g^{ac} at $V_{sd}^{ac} = 8$ V. E) Resonance frequency spectra
 193 of a 160- μm -long SCD-based cantilever transducer measured *via* the electrical readout system

194 from 25 °C to 500 °C at $V_{sd}^{ac} = 3$ V and $V_g^{ac} = 7$ V. F) Resonance frequencies and Q factors as a
 195 function of temperature.

196

197 The measurement setup for the on-chip sensing and actuation of the SCD cantilevers
 198 through an electrical system has been previously described (**Figure 1a**). The resonance
 199 frequency spectra of a 160- μ m-long SCD-based oscillator were customized by changing V_{sd}^{ac} to
 200 $V_g^{ac} = 3$ V at 25 °C, as shown in **Figure 2a**. The resonance frequency spectrum shifted downward
 201 as V_{sd}^{ac} increased, whereas the resonance frequency amplitude increased with V_{sd}^{ac} . The reduction
 202 in resonance frequency, which is known as the “softening” of the SCD-based oscillator, may
 203 be attributed to two reasons: 1) the existence of an electric field force gradient and 2) Joule
 204 heating from the S–D electrodes. When an external electric field V_{sd}^{ac} is applied, the resonance
 205 frequency of the cantilever oscillator can be expressed as $f \approx f_0 + \alpha(V_{sd}^{ac})^2 / (mf_0)$,^[59] where α is the
 206 coefficient related to the SCD polarizability and electric field gradient, f_0 is the resonance
 207 frequency of the oscillator without an electric field force, and m is the oscillator mass. The
 208 resonance frequency exhibits a square relationship with V_{sd}^{ac} , as shown in **Figure S3**
 209 (**Supporting Information**). Furthermore, the inset of **Figure S3 (Supporting Information)**
 210 shows that the ratio of the resonance frequency variation ($\Delta f = f - f_0$) to f_0 increases linearly with
 211 $(V_{sd}^{ac})^2$. Meanwhile, the local temperature of the SCD cantilever increases with V_{sd}^{ac} , which
 212 decreases the effective Young’s modulus and thus induce a downward shift of the resonance
 213 frequency. The function of the resonance frequency shift with the temperature coefficient of
 214 Young’s modulus is expressed as^[60]

$$215 \quad \frac{\Delta f}{f} \approx \frac{1}{2} \frac{\Delta E}{E} \approx \frac{1}{2} \alpha_E \frac{dT}{dW} W \propto (V_{sd}^{ac})^2, \quad (6)$$

216 wherein $\alpha_E = dE/(EdT)$; and W is the input electrical energy, which is proportional to $(V_{sd}^{ac})^2$.
 217 Thus, $\Delta f/f$ exhibits a linear relationship with $(V_{sd}^{ac})^2$. The exact reason for the downward shift of
 218 the resonance frequency of the cantilever oscillator is yet to be confirmed. The plot of the Q
 219 factor vs. V_{sd}^{ac} is presented in **Figure 2b**, which shows that the Q factor decreases as V_{sd}^{ac} increases.

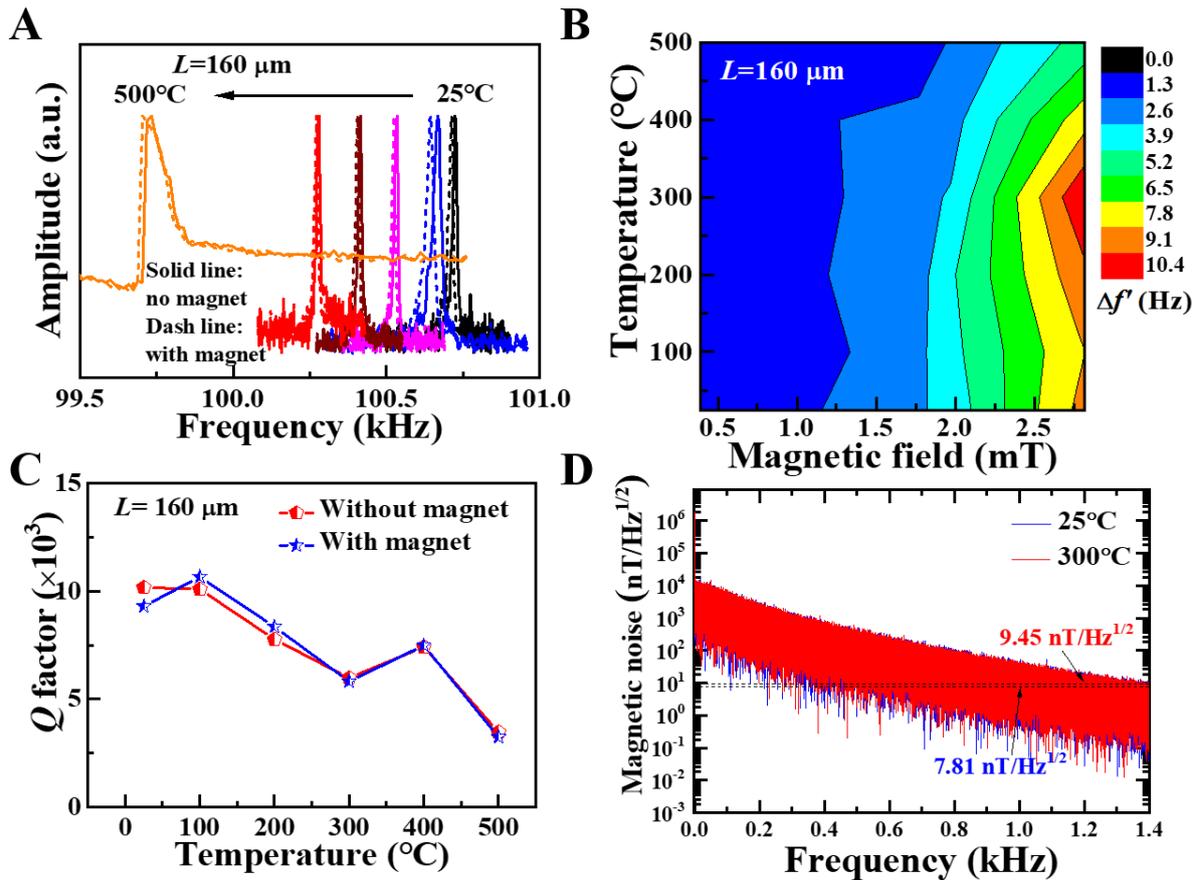
220 A more accurate analysis should consider the thermal mismatch between diamond and FeGa,
 221 which does not affect the magnetic sensitivity for a certain S–D voltage.

222 The resonance frequency spectra of the SCD-based resonator were characterized by
 223 varying V_g^{ac} at $V_{sd}^{ac} = 8$ V and room temperature (**Figure 2c**). The resonance frequency shifted
 224 downward as V_g^{ac} increased, as shown in **Figure S3 (Supporting Information)**. For a cantilever
 225 beam, the resonance frequency is determined by the uniaxial compressive stress, σ of the
 226 cantilever beam, which is expressed as^[61]

$$227 \quad f = f_0 \left(1 + 0.295 \frac{\sigma L^2}{Et^2} \right)^{1/2} \quad (7)$$

228 According to **Equation 2**, σ can be increased by adopting a higher value of V_g^{ac} . Thus, the
 229 decrease in the resonance frequency with a higher V_g^{ac} indicates that σ is a tension stress. This
 230 is different from the case of the optical readout without applying an S–D voltage. The Q factor
 231 shows a weak dependence on V_g^{ac} (**Figure 2d**). The thermal stability of the resonance
 232 performance of the SCD-based oscillator was examined as the temperature increased from
 233 25 °C to 500 °C. The temperature dependence of the resonance frequency spectra of the SCD-
 234 based oscillator is shown in **Figure 2e**. V_{sd}^{ac} and V_g^{ac} were fixed at 3 and 7 V, respectively. The
 235 temperature increase resulted in a decrease in the effective Young's modulus of the multilayer
 236 structure, which caused a downward shift in the resonance frequency (**Figure 2f**). Alternatively,
 237 the temperature coefficient of the resonance frequency (TCF) was used to demonstrate the
 238 thermal stability of the SCD-based oscillator (**Figure S4, Supporting Information**). The TCF
 239 of SCD-based oscillators with various lengths can remain lower than 13 ppm/K, which is
 240 superior to that of Si with a value of 35 ppm/K.^[62] The Q factor of the SCD-based oscillator
 241 decreased at high temperatures but remained as high as 1500 even at 500 °C.

242 **2.5 Magnetic transducing at high temperatures**



243
 244 **Figure 3.** High-temperature magnetic transducing performance through on-chip actuation and
 245 sensing. A) Resonance frequency shift of a 160- μm -long SCD-based cantilever transducer as a
 246 function of the measurement temperature at a magnetic field of 2.82 mT, and at $V_{sd}^{ac} = 4\ \text{V}$ and
 247 $V_g^{ac} = 7\ \text{V}$ from 25 °C to 500 °C. The peak amplitude of the etch spectrum is normalized. B)
 248 Resonance frequency shifts of the magnetic transducer vs. the measurement temperature at
 249 different magnetic fields. C) Q factor variations of the magnetic transducer vs. temperature
 250 without and with applying a magnetic field of 2.82 mT. D) Magnetic noise spectra of the
 251 magnetic transducer at 25 °C and 300 °C.

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Based on the high thermal stability of SCD-based cantilevers with the on-chip actuation and sensing structure, the magnetic transducing of the SCD-based magnetic transducers from 25 °C to 500 °C was realized through the ΔE effect. The dependence of the resonance frequency shift on the magnetic field was utilized to indicate the magnetic sensitivity of the SCD-based transducer. The magnetic sensitivity is defined as $\Delta f' = |f_{r0} - f_{rH}|$, where f_{rH} and f_{r0} represent the resonance frequencies of the SCD-based transducer with and without the magnetic field, respectively. **Figure 3a** shows the resonance frequency spectra shift of the 160- μm -long SCD-

260 based magnetic transducer caused by applying a magnetic field of 2.82 mT with the temperature
 261 increasing from 25 °C to 500 °C. The resonance frequency shifted as a function of the magnetic
 262 fields tuned via temperature (**Figure 3b**). The resonance frequency shift increased with the
 263 magnetic field. The SCD-based magnetic transducer with on-chip actuation and sensing
 264 exhibited a stable magnetic sensitivity of 3.2 Hz/ mT at various temperatures. Therefore, the
 265 on-chip SCD MEMS magnetic sensor with all-electrical actuation and sensing is robust at high
 266 temperatures up to 500 °C. Another SCD-based transducer demonstrates similar magnetic
 267 sensing performances (**Figure S5, Supporting Information**). To some extent, the Q factors of
 268 the SCD-based magnetic transducer decreased as temperature increased (**Figure 3c**). However,
 269 the overall magnetic sensing performance did not change significantly as the temperature
 270 increased. In addition, the magnetic noise spectra resulting from the thermomechanical noise
 271 of the SCD-based magnetic transducer were measured at 25 °C and 300 °C, as shown in **Figure**
 272 **3d**. The magnetic noise levels of the SCD-based magnetic transducer reached a low level of
 273 7.81 nT/Hz^{1/2} at 25 °C and 9.45 nT/Hz^{1/2} at 300 °C. For the MEMS magnetic transducer with
 274 the oscillator structure, the intrinsic magnetic noise (b_n) can be expressed as^[63, 64]

$$275 \quad b_n = \frac{1}{2} \mu_0 \frac{dH}{df} \sqrt{\frac{2\pi k_B T f_{r0}}{QV\sigma'}} b_n, \quad (8)$$

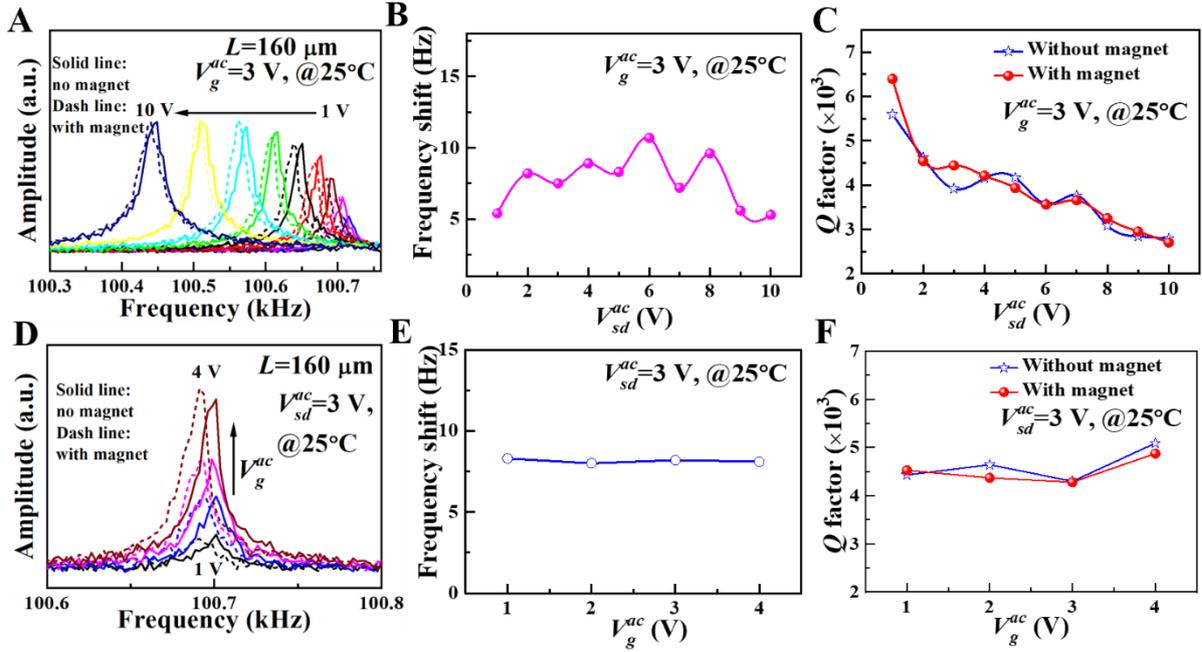
276 which is utilized to predict the theoretical magnetic noise at the resonant frequency f_{r0} . Here,
 277 $\mu_0(dH/df)$ is the magnetic sensitivity of the magnetic transducer, T the temperature, and V the
 278 device volume. The stress, σ' , is calculated from f_{r0} , which is discussed in our previous
 279 publication.^[27] Based on the magnetic sensing performance of the 160- μ m-long on-chip
 280 magnetic transducer, the intrinsic magnetic noises of the magnetic sensor were estimated as
 281 0.632 nT/Hz^{1/2} at 25 °C, 0.825 nT/Hz^{1/2} at 300 °C, and 1.09 nT/Hz^{1/2} at 500 °C. Additionally,
 282 the Allan deviation of the SCD-based magnetic transducer was investigated (**Figure S6,**
 283 **Supporting Information**). The minimum fluctuation of the resonance frequency up to 300 °C
 284 was 2.3×10^{-6} . Based on the magnetic sensitivity, the minimum detectable magnetic fields for

285 the SCD-based magnetic transducer were calculated to be 2.02×10^{-11} T (20.2 pT) and 3.47×10^{-11} T (34.7 pT) at 300 K and 773 K, respectively. Meanwhile, based on the stable magnetic
 286 11 T (34.7 pT) at 300 K and 773 K, respectively. Meanwhile, based on the stable magnetic
 287 sensitivity, high Q factors result in low magnetic noise levels. To improve the magnetic
 288 sensitivity of the SCD-MEMS magnetic transducer, smaller thickness of tens of nanometers in
 289 SCD resonators is preferred. However, for high-speed response, high-frequency resonators with
 290 shorter length (i.e. micrometer scale) are desirable. A larger thickness of the FeGa film is
 291 favorable as well, but a trade-off with the Q factor should be considered. The high-temperature
 292 magnetic sensing performances of various representative high-temperature magnetic sensors
 293 were compared with those of the present sensor in terms of magnetic sensitivity, magnetic noise,
 294 and thermal stability, as summarized in **Table 1**. The on-chip magnetic sensor in this study
 295 exhibits superior sensitivity, lower noise level, and higher thermal reliability compared with
 296 other magnetic sensors.

297 **Table 1.** High-temperature sensing performance comparison of various high-temperature
 298 magnetic sensors.

Magnetic sensor	Materials	Magnetic sensitivity	Noise level	Operating temperature	Stable operating duration	Ref.
AMR	Si-based	--	~ 2.6 nT/Hz ^{1/2}	498 K	>2000 h	[65]
Hall	Si	--	>82 nT/Hz ^{1/2}	673 K	--	[66]
Hall	AlGaN/ GaN	--	$35 \mu\text{T}/\sqrt{\text{Hz}^{1/2}}$	873 K	--	[67]
Hall	4H-SiC	80 V/(A·T)	--	770 K	--	[68]
Fluxgate	Cu coil	--	0.79 nT/Hz ^{1/2}	523 K	>100 h	[26]
MEMS	FeGa/Ti/ SCD	3.2 Hz/mT	9.45 nT/Hz ^{1/2}	573 K	>100 h	This study

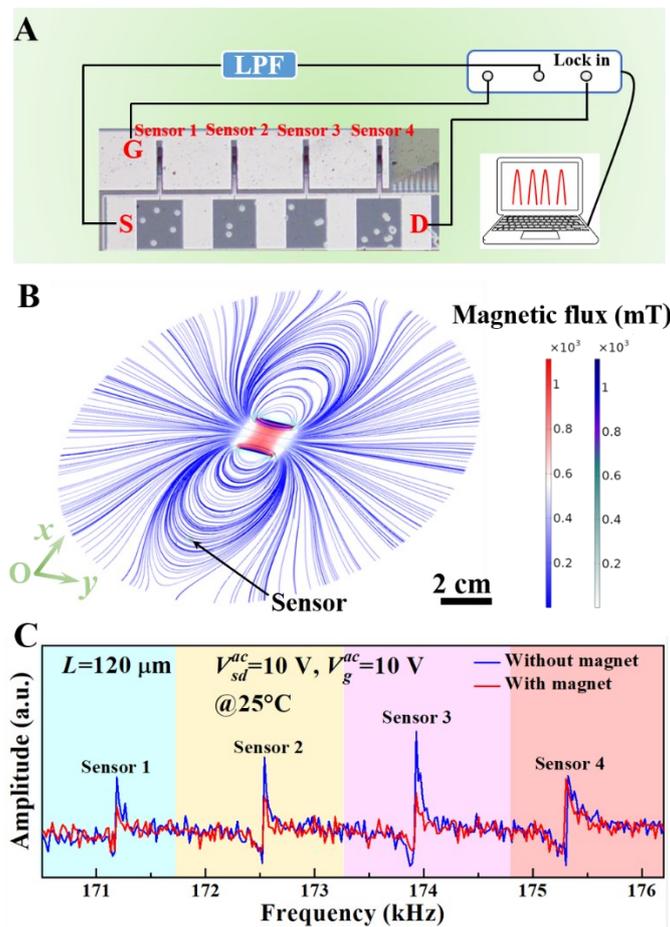
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300
 301 **Figure 4.** Magnetic transducing performances with changing V_{sd}^{ac} and V_g^{ac} at room temperature.
 302 A) Resonance frequency spectra of a 160 μm -long SCD-based magnetic transducer response to
 303 a magnetic field of 2.82 mT by changing V_{sd}^{ac} at $V_g^{ac} = 3$ V. B) Tuning of resonance frequency
 304 shift of the magnetic transducer *via* V_{sd}^{ac} under a magnetic field of 2.82 mT at $V_g^{ac} = 3$ V. C)
 305 Dependence of Q factors of the magnetic transducer on V_{sd}^{ac} without and with a magnetic field
 306 of 2.82 mT. V_g^{ac} is fixed at 3 V. D) Resonance frequency spectra of the magnetic transducer
 307 response to a magnetic field of 2.82 mT by changing V_g^{ac} at $V_{sd}^{ac} = 3$ V. E) Resonance frequency
 308 shifts of the magnetic transducer as a function of V_g^{ac} under a magnetic field of 2.82 mT at V_{sd}^{ac}
 309 = 3 V. F) Variation in Q factors of the magnetic transducer as V_g^{ac} without and with a magnetic
 310 field of 2.82 mT. V_{sd}^{ac} is fixed at 3 V.

311
 312 The effects of V_{sd}^{ac} and V_g^{ac} on the the magnetic sensing performance of the on-chip magnetic
 313 transducer are investigated. **Figure 4a** shows the dependences of the resonance frequency
 314 spectra shift of the SCD-based magnetic transducer on V_{sd}^{ac} with or without applying a magnetic
 315 field ($H = 2.82$ mT) at 25 $^{\circ}\text{C}$ and $V_g^{ac} = 3$ V. The solid and dashed lines represent the resonance
 316 frequency spectra without and with the application of the magnetic field, respectively. Although
 317 the resonance amplitude increased with V_{sd}^{ac} , the resonance frequency of the on-chip magnetic
 318 transducer was barely affected by V_{sd}^{ac} (**Figure 4b**) under a magnetic field. The Q factors of the
 319 on-chip magnetic transducer without and with the magnetic field decreased as V_{sd}^{ac} increased

320 (Figure 4c). The possible reasons have been discussed in the previous section. Thus, a suitable
 321 V_{sd}^{ac} should be selected with regard to two aspects: (1) a sufficient voltage to achieve a high
 322 signal readout and (2) minimal impact on the Q factor. Figure 4d shows the effect of V_g^{ac} on the
 323 resonance frequency shift of the on-chip transducer with or without the application of a
 324 magnetic field ($H = 2.82$ mT) at 25°C and $V_{sd}^{ac} = 3$ V. Similarly, the amplitude of the resonance
 325 frequency with and without the application of the magnetic field increased with V_g^{ac} , as shown
 326 in Figure 4e. V_g^{ac} did not significantly affect the resonance frequency shift or Q factor when the
 327 magnetic field was applied, as shown in Figures 4e and f.



328
 329 **Figure 5.** Magnetic transducing of a transducer array. A) Measurement setup for an SCD-based
 330 magnetic transducer array with the on-chip actuation and sensing configuration. The length and
 331 width of each cantilever sensor were 120 and $10\ \mu\text{m}$, respectively. B) The magnetic flux density
 332 in the xoy plane of a cylindrical magnet is simulated using the COMSOL software. The
 333 magnetization of this magnet merely occurs in the y -axis direction, showing a magnetic
 334 susceptibility of $1032000\ \text{A/m}$. The height and radius of the cylindrical magnet were 2 and 1

335 cm, respectively. C) Resonance frequency spectra shifts of the magnetic transducer array due
336 to the application of a 2.82 mT magnetic field at $V_{sd}^{ac} = 10$ V and $V_g^{ac} = 10$ V @25 °C. The
337 magnetic transducer array comprised four SCD-based magnetic sensors.

338

339 Finally, we demonstrate an SCD-based magnetic transducer array comprising four on-chip
340 magnetic transducers integrated on the same chip for magnetic transducing with all-electrical
341 actuation and sensing. **Figure 5a** shows an on-chip SCD-based magnetic transducer array.
342 COMSOL software was utilized to simulate the magnetic flux distribution of a two-dimensional
343 plane of a cylindrical magnet (**Figure 5b**). Owing to the independent resonance vibration of
344 each magnetic transducer, the parallel signal readout of the four magnetic transducers was
345 realized. The resonance frequency spectra of the magnetic transducer array exhibited four peaks
346 without and with the application of a magnetic field of 0.28 mT, respectively, as depicted in
347 **Figure 5c**. The resonance frequencies shifted downward in the magnetic transducer array
348 because of the ΔE effect. A view of the resonance frequency shift with the application of a
349 magnetic field is shown in **Figure S7 (Supporting Information)**. Alternatively, applying a
350 magnetic field exhibited a weak effect on the Q factor of each magnetic sensor in the magnetic
351 transducer array (**Figure S7, Supporting Information**). The successful realization of the
352 magnetic sensing of the SCD-based magnetic transducer array is a first step toward the
353 development of robust magnetic image sensors with high sensitivity and spatial resolution.

354

355 3. Conclusion

356 In summary, we proposed and demonstrated an all-electrical on-chip diamond MEMS
357 magnetic sensor by integrating magnetostrictive FeGa with an SCD MEMS resonator. The
358 magnetostrictive FeGa film functioned as an actuation electrode, a sensing head for magnetic
359 fields, and an electrical readout unit. The SCD-based MEMS magnetic transducer exhibited
360 high-temperature operation up to 500 °C with a high-sensitivity of 3.2 Hz/mT and a low noise

361 level of $9.45 \text{ nT/Hz}^{1/2}$ at $300 \text{ }^\circ\text{C}$. The minimum fluctuation of the resonance frequency reached
362 1.9×10^{-6} at room temperature and 2.3×10^{-6} at $300 \text{ }^\circ\text{C}$. The prototype SCD-based MEMS
363 magnetic transducer array was developed with the achievement of parallel signal readout. The
364 magnetic sensing performance can be further enhanced via nanoscale size design,^[69] a high
365 quality factor,^[70] and a large magneto-strictive thin film.^[69, 71] The current study successfully
366 demonstrated the integration of SCD-based MEMS magnetic transducers with electronics,
367 which serves as a foundation toward the development of magnetic image sensors with high
368 sensitivity, reliability, and tunable spatial resolution.

369

370 **4. Experimental section**

371 ***4.1 Fabrication of on-chip SCD-based cantilever transducers***

372 The fabrication of the SCD cantilevers was begun from the homoepitaxial layers grown
373 on the high-pressure high-temperature (HPHT) SCD substrates. Before the diamond growth,
374 the HPHT SCD substrates were orderly cleaned in boiling mixture acids ($\text{H}_2\text{SO}_4+\text{HNO}_3$),
375 acetone, ethanol, and deionized water. Then, the cleaned HPHT SCD substrates were undergone
376 the implantation treatment of carbon ions at an energy of 180 keV and a dose of 10^{16} cm^{-2} . The
377 diamond epilayers were grown on the HPHT SCD substrates *via* a microwave chemical vapor
378 deposition (MPCVD) facility with growth parameters of a methane concentration of 1% , a
379 hydrogen flow of 500 sccm , a microwave power of 1000 W , a substrate temperature of 880°C
380 and a growth duration of 2 h . During the diamond growth, a 200 nm -thick graphite-like layer
381 resulted from the ion implantation was formed under the diamond surface, which was acted as
382 a sacrificial layer to produce the cantilever structure. The structure of the graphite-like layer
383 was characterized through a transmission electron microscopy (TEM) technique, as shown in
384 detail in our pervious works.^[72, 73] The existence of the graphite-like layer had little impact on

385 the crystal quality of the SCD epilayer, as disclosed by Raman spectroscopy mapping (**Figure**
386 **S8, Supporting Information**). The graphite-like layer was removed through wet or dry etching
387 to release the SCD cantilevers. Thus, the graphite-like layer has weak influence on the sensing
388 performance of the SCD-based magnetic transducers. However, the diamond at the bottom of
389 the cantilever was defective due to the ion implantation. To eliminate this damage, the SCD
390 samples were annealed at 1100°C for 3 h in an ultrahigh vacuum condition ($\sim 10^{-7}$ Pa). However,
391 we could not identify the damage induced by the ion-implantation through TEM and Raman.
392 By contrast, the Q factors of the SCD cantilevers were improved after annealing at 1100°C
393 (**Figure S9, Supporting Information**). A laser photolithographic approach was utilized to
394 pattern the SCD samples and fabricate the SCD cantilevers.^[32]

395 A further laser photolithography process was utilized to pattern the on-chip SCD
396 cantilevers with the actuation and sensing structure. A 2 nm-thick Ti film followed by a 90 nm-
397 thick FeGa film was deposited on the SCD cantilevers by a magneto sputtering system. The
398 FeGa film was regarded as actuation electrode, magnetic transducing component, and electrical
399 readout unit. The growth conditions of the Ti and FeGa films were: a Ar flow of 10 sccm, a
400 working pressure of 1 Pa, a sputtering power of 100 W, and room temperature. Alternatively, a
401 1 nm-thick Ti film followed by a 7 nm-thick Au film was deposited on SCD cantilevers as the
402 source, drain, and gate electrodes by an e-beam evaporator system. The SCD cantilever
403 configuration with an actuation and sensing configuration was confirmed by an optical
404 microscope system.

405 ***4.2 Optical and electrical readout of the mechanical resonance***

406 The mechanical resonance properties of the SCD cantilevers without and with the
407 deposition of films including FeGa/Ti films and Au electrodes were analyzed *via* an optical
408 readout system with the Laser Vibrometry. The gate electrode connected to a RF signal was
409 used to actuate the SCD cantilevers. The optical signal reflected from the vibration of the SCD

410 cantilevers was read out by a lock-in amplifier. The magnetic transducing performance of the
411 SCD-based magnetic transducers with the actuation and sensing structure were measured by an
412 electrical readout system. The G electrode was connected to a radio-frequency (RF) signal with
413 an amplitude of V_g^{ac} and a frequency of ω to actuate the cantilevers. Another RF signal with an
414 amplitude of V_{sd}^{ac} and a frequency of $\omega + \Delta\omega$ was applied to the S-D electrode to capture the
415 vibrational signal. The displacement of the cantilevers led to the variation in the resistance of
416 the S-D electrode. A reference signal, $\Delta\omega$ of 5 kHz was utilized to readout the electrical signal.
417 The magnetic fields were applied by the different magnets to accomplish the magnetic
418 transducing measurement. A heater below the magnetic transducer was utilized to control the
419 temperatures from room temperature to high temperatures. The measurements were performed
420 in a vacuum chamber with a pressure lower than 10^{-3} Pa.

421 **Supporting Information**

422 Supporting Information is available from the Wiley Online Library or from the author.

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428

429 **Conflict of Interest**

430 The authors declare no conflict of interests.

431

432 **Data Availability Statement**

433 The data that support the findings of this study are available on request from the corresponding
434 author.

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