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1 Impact of hydrophobic modification on biocompatibility of Alaska pollock gelatin microparticles

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Abstract

This study investigates the impact of hydrophobic modification on the immunogenicity, cytotoxicity, and inflammatory response of Alaska pollock gelatin (ApGln) microparticles (MPs). Gelatin, known for its inherent biocompatibility, was modified with decyl group (C10) to explore potential alterations in its interaction with the immune system. Immunogenicity was evaluated through the measurement of material-specific IgM and IgG responses, indicating no significant increase post-modification. Cytotoxicity against Caco-2 cell lines and NF-kB-mediated LPS-induced inflammation were also assessed, revealing no exacerbation by the modified MPs. Furthermore, C10-modification with different types of linkage such as secondary amine and amide structure did not influence immune reactivity. These findings suggest that C10-modification maintains the non-immunogenicity and biocompatibility of gelatin MPs, supporting their potential use in biomedical applications.

Keywords: Alaska pollock gelatin microparticle, decyl-group modification, immunogenicity, biocompatibility

1. Introduction

Gelatin, a versatile biopolymer derived from collagen, has been widely used in various industries, including food, pharmaceutical and cosmetics, owing to its remarkable properties that enhance viscosity, texture, and stability of products [1]. Traditionally, gelatin has been sourced primarily from pig skins, bovine hides, and bones. However, recent attention has shifted towards alternative sources, particularly fish and fish by-products, such as fish bones and skins, as promising biomaterials for gelatin production [2]. The distinctive characteristics of fish gelatin, such as its lower gelling and melting points compared to gelatin derived from porcine or bovine sources [3], enable its use in applications requiring higher fluidity at room temperature.

Alaska pollock gelatin (ApGltN) has been explored as a basic material for biodegradable surgical sealants due to its low transition temperature, low imino acids content and low viscosity [4]. Introduction of several hydrophobic groups such as cholesterol, alkyl chains with various length have been demonstrated to enhance interfacial strength under wet conditions [5–7]. Among these modifications, the incorporation of the decyl group (C10) onto ApGltN has been highlighted for its notable enhancement of interfacial strength with blood vessels [6]. Interestingly, microparticles formed by the self-assembly of C10-modified ApGltN swelled into a stable hydrogel layer in physiological saline, which was demonstrated to protect the wound surface and facilitate the tissue regeneration process in wound healing models [7]. Notably, in addition to internal gastrointestinal tissue, efficacy in preventing postoperative adhesion on duodenum serosal tissue was also demonstrated [8].

Given that most C10 modifications were targeted to the primary amine groups of ApGltN, the exposure of primary amine groups may have implications for immunogenicity and inflammatory response. For example, primary amines on polymers have been reported to form hydrogen bonds and electrostatic interactions with phosphate groups in lipids, disrupting the organization of lipid bilayers and potentially increasing toxicity [9]. Furthermore, *in vivo* toxicity associated with cationic nanoparticles such as chitosan and bPEI nanoparticles, which induce complement activation and Toll-like receptor 4 (TLR-4) activation respectively, underscores the importance of understanding the impact of primary amine exposure. Interestingly, modifying primary amines to secondary and tertiary amines has shown promise in mitigating these adverse effects [10], suggesting a potential strategy for enhancing biocompatibility and minimizing risk of potential inflammation in biomedical applications.

Thus, in this study, C10-modification was performed on amine groups in ApGltN with different types of linkage formation: amide (C10-am-ApGltN) and secondary amine (C10-sa-ApGltN), prior to microparticle fabrication, allowing a comprehensive evaluation of the immunogenicity, cytotoxicity and inflammatory response associated with these microparticles. By investigating the interactions between these modified microparticles and biological systems, insights can be gained into their biocompatibility post-modification and potential suitability for biomedical applications.

70 2. Materials and Methods

71 2.1 Materials

72 Alaska pollock gelatin (ApGtln, molecular weight (MW) = 34,352 Da, amine group content: 364 $\mu\text{mol/g}$ and MW
73 = 34,323 Da, amine group content: 355 $\mu\text{mol/g}$) was purchased from Nitta Gelatin Inc. (Osaka, Japan). Decanal
74 and decanoic anhydrate were obtained from Tokyo Chemical Industry Co., Ltd. (Osaka, Japan). Ethanol and 2-
75 picoline borane were purchased from Junsei Chemical Co., Ltd. (Tokyo, Japan). Dulbecco's Modified Eagle
76 Medium (DMEM), Antibiotic-Antimycotic Mixed Stock Solution, MEM Non-Essential Amino Acids Solution,
77 Dulbecco's Phosphate-buffered Saline (DPBS) and dimethyl sulfoxide (DMSO) were purchased from Nacalai
78 Tesque, Inc. (Kyoto, Japan). Fetal bovine serum (FBS) was purchased from Nichirei Bioscience Inc. (Tokyo,
79 Japan). Trypsin-EDTA was purchased from Gibco (Waltham, MA, USA). Cell Counting Kit-8 (CCK-8) was
80 purchased from Dojindo Laboratories (Kumamoto, Japan). Sodium carbonate, 4-Nitrophenyl phosphate disodium
81 salt hexahydrate, albumin from mouse serum (MSA), albumin from chicken egg white (OVA), lipopolysaccharide
82 (LPS) from *Escherichia coli* O111:B4 and TWEEN[®] 20 were purchased from Sigma-Aldrich (Saint Louis, MO,
83 USA). Sodium hydrogen carbonate, magnesium chloride hexahydrate, G418 sulfate and sulfuric acid were
84 purchased from FUJIFILM Wako Pure Chemical Corporation (Osaka, Japan). Anti-mouse horseradish peroxidase
85 (HRP)-conjugated IgM and IgG were purchased from Bethyl Laboratories, Inc (Montgomery, TX, USA). 3, 3',
86 5, 5' tetramethyl benzidine (TMB) was purchased from BioLegend, Inc. (San Diego, CA, USA).

88 2.2 Synthesis of C10-sa-ApGtln

89 C10-sa-ApGtln was synthesized following a previously established method [11, 12]. In brief, ApGtln (50 g) was
90 dissolved into 175 mL of ultrapure water at 50 °C under continuous stirring at 400 rpm. Subsequently, 35 mL of
91 ethanol and 35.5 mmol of decanal (two equivalent molar ratio of amine groups in ApGtln) dissolved into ethanol
92 were added into the ApGtln solution, followed by 1 hour of stirring at 50 °C. Then, 53.3 mmol of 2-picoline borane
93 (1.5 equivalent molar ratio of decanal), used as a reductant, was added to the ethanol solution under continuous
94 stirring at 400 rpm. The resulting solution had a 20 w/v% ApGtln concentration (water: ethanol = 175:75 (mL)).
95 After stirring the reaction for 17 hours, the solution was dropped into 2,500 mL of chilled ethanol (maintained at
96 -7 to 4 °C) to induce precipitation. The precipitate was washed three times with 1,250 mL of ethanol to remove
97 residual decanal and 2-picoline borane, then vacuum dried overnight (< 3 mbar) to obtain C10-sa-ApGtln powder.
98 The degree of substitution (DS) was measured by TNBS method where residual amine groups were labeled by
99 2,4,6-trinitrobenzene sulfonic acid (TNBS) to measure the absorbance [13].

101 2.3 Synthesis of C10-am-ApGtln

102 C10-am-ApGtln was synthesized through a reaction with primary amine and decanoic anhydrate. Briefly, ApGtln
103 (10 g) was dissolved in 35 mL of 0.1 M phosphoric acid buffer solution (pH 8.0) at 50 °C with continuous stirring
104 at 400 rpm. Subsequently, 7.06 mmol of decanoic anhydrate (2-equivalent molar ratio of amine groups in ApGtln)
105 was dissolved in 15 mL of ethanol and added into the ApGtln solution. The resulting solution had a 20 w/v%
106 ApGtln concentration (water: ethanol = 35:15 (mL)). After stirring for 1 hour, the obtained solution was dropped
107 into 500 mL of iced ethanol (maintained at -7 to 4 °C) to reprecipitate. The precipitate was washed three times

108 with 250 mL of ethanol to remove residual decanoic acid. The washed precipitate was dissolved in a water/ethanol
109 mixture (35/15 mL) and then dialyzed against 2 L of a water/ethanol mixture at a ratio of 7/3 (v/v) for 2 days at
110 room temperature. The dialyzed solution was freeze dried to obtain C10-am-ApGln powder. The DS was
111 measured by TNBS method.

112 113 **2.4 Preparation and characterization of C10-sa-MPs and C10-am-MPs**

114 C10-sa- and C10-am-MPs were prepared using the coacervation method, following a previous method [7, 8, 12,
115 14]. In this process, a poor solvent for C10-sa- and C10-am-ApGln was used to induce coacervation. C10-sa- or
116 C10-am-ApGln was dissolved in ultrapure water at a concentration of 5 w/v%. An equal volume of ethanol,
117 serving as a poor solvent, was added dropwise to the ApGln solution, inducing the formation of a coacervate. The
118 resulting coacervate solutions were freeze dried to remove water and ethanol. Subsequently, thermal treatment at
119 150 °C for 3 hours under vacuum conditions (< 3 mbar) was applied to facilitate the formation of chemical bonds
120 between C10-sa- or C10-am-ApGln molecules. Org-MPs derived from Org-ApGln, non-modified Alaska
121 pollock gelatin, were prepared using the same procedure. The obtained MPs were examined using scanning
122 electron microscopy (SEM; JCM- 7000, JEOL, Japan) and the particle diameter was determined using Image J
123 software.

124 125 **2.5 Mice**

126 Female Balb/c mice (6 weeks old) were purchased from Kyudo Co. Ltd. (Saga, Japan) and acclimatized for one
127 week before the commencement of experiments. All animals were housed under standard laboratory conditions
128 on a 12-hour light-dark cycle. During the acclimatization and experimental periods, mice were provided with CE-
129 2 (CLEA Japan, Inc.) and had *ad libitum* access to water. The diet and water were replaced and replenished as
130 needed to ensure the well-being of the animals. Experiment was conducted with approval from the Institutional
131 Animal Care and Use Committee of Kyushu University.

132 133 **2.6 Immunogenicity of MPs**

134 Female Balb/c mice were randomly divided into groups of five. Each group received four consecutive
135 subcutaneous injections per week with the following substances: Org-MPs (0.4 mg/mL), C10-am-MPs (0.4
136 mg/mL), C10-sa-MPs (0.4 mg/mL), MSA (0.4 mg/mL) and OVA (0.4 mg/mL), respectively. Following the final
137 injection, mice sera were collected one week later for analysis.

138 139 **2.7 Enzyme-Linked Immunosorbent Assay (ELISA)**

140 ELISA was conducted following the protocol published by Li et al. [15] with slight modifications. In brief, ELISA
141 plates were coated with 100 µL of sample solution (10 µg/mL), containing the substances to be tested (Org-MPs,
142 C10-am-MPs, C10-sa-MPs, MSA and OVA, respectively), prepared in 0.1 M sodium carbonate buffer (pH 10.5)
143 and incubated at 4°C overnight. Following the coating procedure, plates underwent five washes with PBS-T and
144 were subsequently blocked with 1% BSA for 1 hour at room temperature. After blocking, plates were washed
145 again five times with PBS-T before being incubated with diluted mice sera (in 1% BSA solution) for 1 hour at

146 room temperature. Following this incubation, plates were washed five times with PBS-T and then incubated with
1 147 diluted HRP-conjugated IgM and IgG (1:50,000) for 1 hour at room temperature. Subsequently, plates were
2 148 washed five times with PBS-T and incubated with TMB substrate for 15 minutes at room temperature. The
3 149 reaction was stopped by adding 0.2 M H₂SO₄ solution. Absorbance was measured at 450 nm with a reference
4 150 wavelength of 570 nm using Infinite® 200 PRO M Plex (Tecan, Switzerland).
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7 152 **2.8 Cell cultures**

10 153 Human colorectal adenocarcinoma (Caco-2) cells were cultured and maintained in complete DMEM,
11 154 supplemented with 10% heat-inactivated FBS, 1% antibiotic-antimycotic mixed stock solution and 1% MEM non-
12 155 essential amino acid solution. RAW264.7 macrophages transfected with secreted alkaline phosphatase (SEAP)
13 156 gene under the transcriptional control of NF-κB responsive promoter, were cultured and maintained in complete
14 157 DMEM, supplemented with 10% heat-inactivated FBS, 1% antibiotic-antimycotic mixed stock solution and 500
15 158 μg/mL G418. All cell lines were cultured at 37°C in a humidified atmosphere of 95% air and 5% CO₂.
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17 160 **2.9 Cytotoxicity of MPs**

18 161 Cytotoxicity against Caco-2 cells was assessed using Cell Counting Kit-8 assay. Briefly, Caco-2 cells were seeded
19 162 at a density of 2 x 10⁴ per well in a 96-well plate and allowed to pre-incubate for 24 hours at 37°C in a 5% CO₂
20 163 atmosphere. Subsequently, the cells were treated with MPs at concentrations ranging from 6.25 to 200 μg/mL or
21 164 with 10% DMSO (v/v) for either 24 hours or 48 hours, at 37°C in a 5% CO₂ atmosphere. MPs solutions were
22 165 prepared by first dispersing it in DPBS, followed by 2-fold serial dilutions using DPBS. After the treatment period,
23 166 CCK-8 was added to each well according to the manufacturer's instruction and incubated for 2 hours at 37°C in
24 167 a 5% CO₂ atmosphere. Absorbance was then measured at 450 nm using Infinite® 200 PRO M Plex (Tecan,
25 168 Switzerland). Cell viability was calculated using the following formula: -
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$$28 \quad \% \text{ viability} = \frac{A_1 - A_0}{A_c - A_0} \times 100$$

29 170 where A₀ is the absorbance value of wells lacking the presence of CCK-8, A₁ is the absorbance value of wells
30 171 containing both samples and CCK-8, and A_c is the absorbance value of wells containing CCK-8 alone, without
31 172 any samples.
32 173

33 174 **2.10 NF-κB-mediated inflammatory response of MPs**

34 175 The NF-κB-mediated inflammatory response of MPs was assessed by quantification of secreted alkaline
35 176 phosphatase (SEAP) activity based on the hydrolysis of para-nitrophenylphosphate (pNPP) into para-nitrophenol
36 177 (pNP), a yellow compound detectable at 405 nm. Briefly, RAW264.7 macrophages transfected with the SEAP
37 178 gene (SEAP-RAW264.7) were seeded at a density of 2 x 10⁴ per well in a 96-well plate and pre-incubated for 24
38 179 hours at 37°C in a 5% CO₂ atmosphere. Subsequently, the cells were treated with MPs at concentrations ranging
39 180 from 2 to 200 μg/mL for 6 hours at 37°C in a 5% CO₂ atmosphere. MP solutions were prepared by first dispersing
40 181 it in DPBS, followed by 10-fold serial dilutions using DPBS. After the 6-hour treatment period, LPS was added
41 182 to each well at a final concentration 20 ng/mL, and the cells were further incubated for 18 hours at 37°C in a 5%
42 183 CO₂ atmosphere. Following incubation, culture supernatants were collected and heated at 65°C for 5 minutes to
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184 inactivate other alkaline phosphatases in the cells and serum [16]. An equal volume of culture supernatant and 4-
185 Nitrophenyl phosphate (1 mg/mL) in substrate buffer (composed of 13.2 mM Na₂CO₃, 35 mM NaHCO₃, 1mM
186 MgCl₂ at pH 9.6 [17]) was mixed and incubated at 37°C for 3 hours in the dark. Absorbance was then measured
187 at 405 nm using Infinite® 200 PRO M Plex (Tecan, Switzerland).
188

189 **2.11 Statistical analysis**

190 Statistical analyses were conducted using GraphPad Prism 9 (La Jolla, CA, USA). One-way ANOVA was
191 employed to assess the significance of means across all groups, followed by Dunnett's multiple comparisons test
192 to compare each mean to the control group. Significance levels were denoted as follows: *P < 0.05, **P < 0.01,
193 ***P < 0.001, ****P < 0.0001.

194 3. Results and Discussion

195 3.1 Characterization of MPs

196 The DS of C10-sa-ApGln and C10-am-ApGln were 47 mol% and 44 mol% against total amount of primary amine.
197 As reported previously, C10-sa-ApGln and C10-am-ApGln were successfully synthesized based FT-IR spectra
198 and ¹H NMR spectra [13]. In the paper, the increased C-H bond stretching peak of -CH₂- structure at 2,927 cm⁻¹
199 in both C10-sa-ApGln and C10-am-ApGln FT-IR spectra compared to Org-ApGln spectra and increased C-H
200 peak at 1.24 ppm in both C10-sa-ApGln and C10-am-ApGln ¹H NMR spectra were confirmed. From these result
201 and literature, the modification of decyl group was considered successful.

202
203 Afterward, three types of microparticles (MPs) were successfully prepared by coacervation method as described
204 previously [7, 8, 12, 14]. Scanning electron microscopy (SEM) observations of all MPs revealed the consistent
205 formation of monodispersed, spherical, and smooth MP structures (Figure 1b-d). The average diameter of MPs
206 prepared by Org-ApGln was approximately 2.26 μm (Figure 1e). However, MPs prepared by C10-sa-ApGln and
207 C10-am-ApGln exhibited a slight increase in average diameter, with a difference of approximately 0.8 μm (Figure
208 1f, g). Through C10 modification, the increase in hydrophobicity of ApGln introduces additional sites for
209 intermolecular interaction within the gelatin matrix. This promotes stronger interactions between ApGln chains
210 and particles, leading to the formation of larger clusters of ApGln molecules and, consequently, resulting in an
211 increase in microparticle size. However, there was no difference in particle size between C10-sa-MPs and C10-
212 am-MPs, indicating that the type of linkage between C10 group and ApGln does not significantly influence the
213 self-assembly process of microparticle formation. This suggest that the overall hydrophobicity of the ApGln,
214 rather than the type of C10 group modification method, is the primary factor that drive the observed change in
215 particle size.

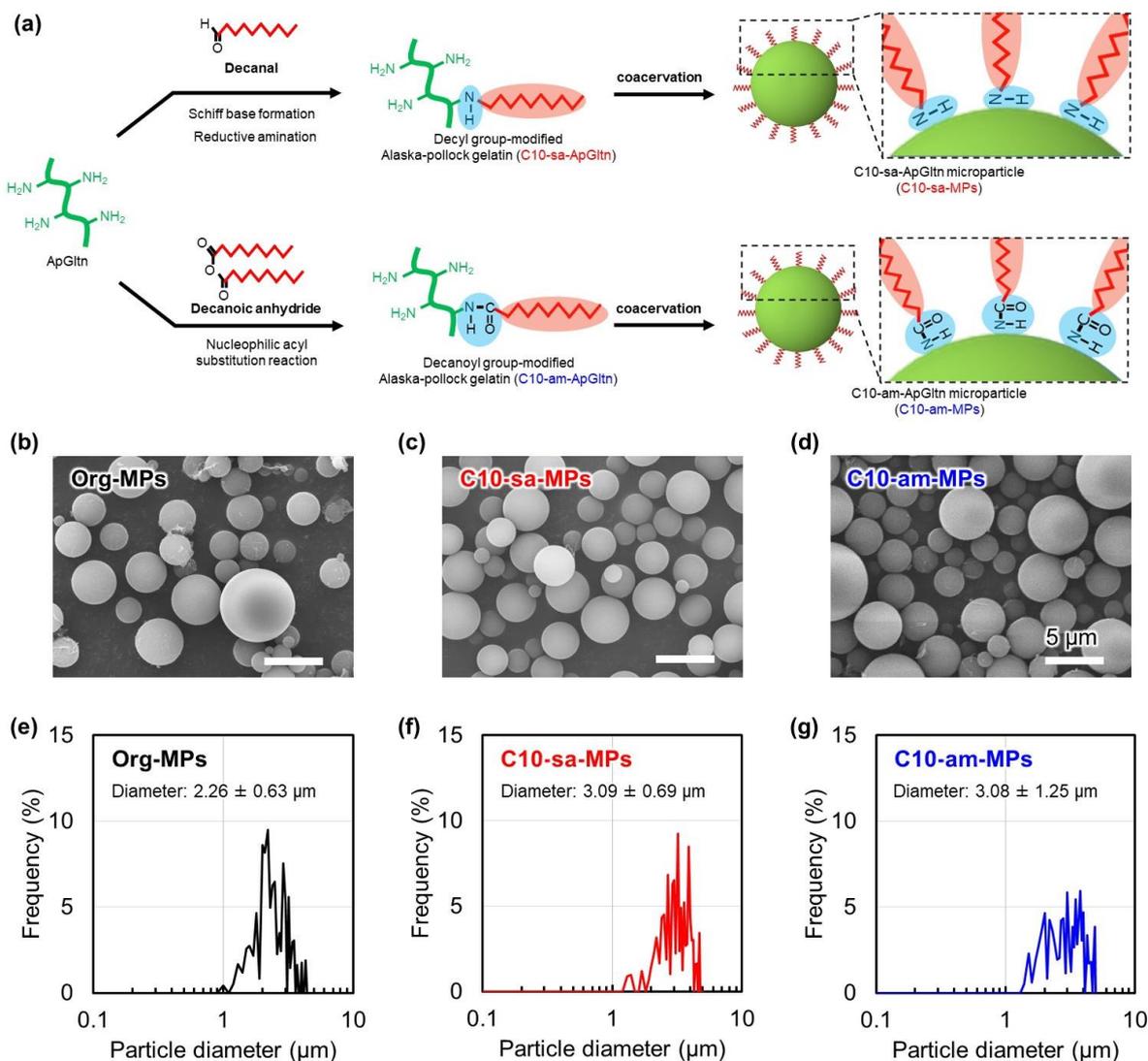


Figure 1: (a) Synthesis of C10-sa-ApGltN and C10-am-ApGltN to prepare C10-sa-MPs and C10-am-MPs. Characterization of Org-, C10-sa-, C10-am-MPs. (b-d) Scanning electron microscopy (SEM) images of Org-, C10-sa-, C10-am-MPs. The scale bars represent 5 μm . (e-g) Particle diameter distribution of Org-, C10-sa-, C10-am-MPs. Particle diameter analysis was performed by ImageJ software. 100 particles were analyzed for each analysis.

3.2 Immunogenicity of MPs

While previous studies have highlighted the superior characteristics of microparticles (MPs) as a surgical sealant, it is crucial to assess their potential risk in triggering unnecessary immune responses. This consideration is especially significant due to the inherent risk associated with polymers, which often induce the production of material-specific antibodies that may compromise their effectiveness in biomedical applications. To evaluate the immunogenicity of MPs, subcutaneous injection in mice was employed. The subcutaneous route was selected based on its relevance, as anti-drug antibodies are frequently associated with drugs administered via this route [18].

To evaluate the production of MPs-specific antibodies, mice received a total of four subcutaneous injections of the respective MPs, administered once per week. Serum samples were collected, and a series of diluted serum samples were used to quantify antibody titers using a sandwich ELISA with plates coated with the respective MPs [15]. In this experiment, ovalbumin (OVA) is used as a positive control due to its well-known immunogenic properties [19], providing a standard reference for evaluating the immunogenicity of all test MPs. Conversely, mouse serum albumin (MSA) was used as negative control as it is a common protein native to mice itself, and its immunogenicity is expected to be minimal [20]. This was confirmed in Figure 2, where OVA induced a high titer of OVA-specific IgG while MSA activity was negligible.

By comparing to OVA treatment group, Org-MPs, which was prepared from unmodified ApGltN, did not induce specific IgM or IgG responses, demonstrating the non-immunogenic nature of ApGltN. Additionally, specific IgG response to C10-modified ApGltN, either at its linkage structures: amide (C10-am-MPs) or secondary amine (C10-sa-MPs), were not observed. While the length of alkyl side chain has been previously demonstrated to confer immunogenicity to peptide vaccine [21], it itself did not induce any immunogenic responses in this study.

On the other hand, in the IgM production evaluation, specific IgM seemed to be detected in mice injected with C10-modified ApGltN. However, similar levels of IgM were also detected in the C10-modified ApGltN-untreated group (Figure S1), suggesting that the observed IgM may be due to nonspecific adsorption and not directly related to the substance itself.

In other words, these results suggest that all tested MPs did not induce targeted antibody responses and are unlikely to induce an immune reaction or sensitization upon exposure.

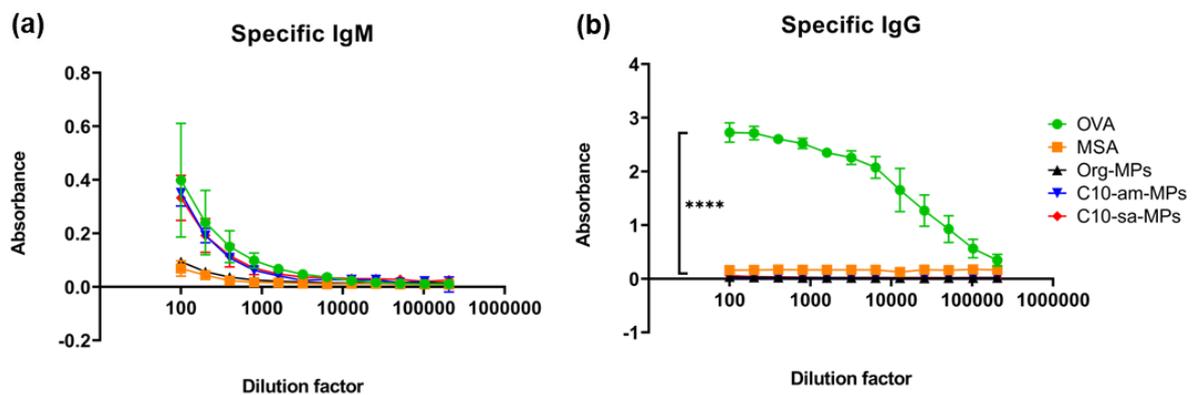
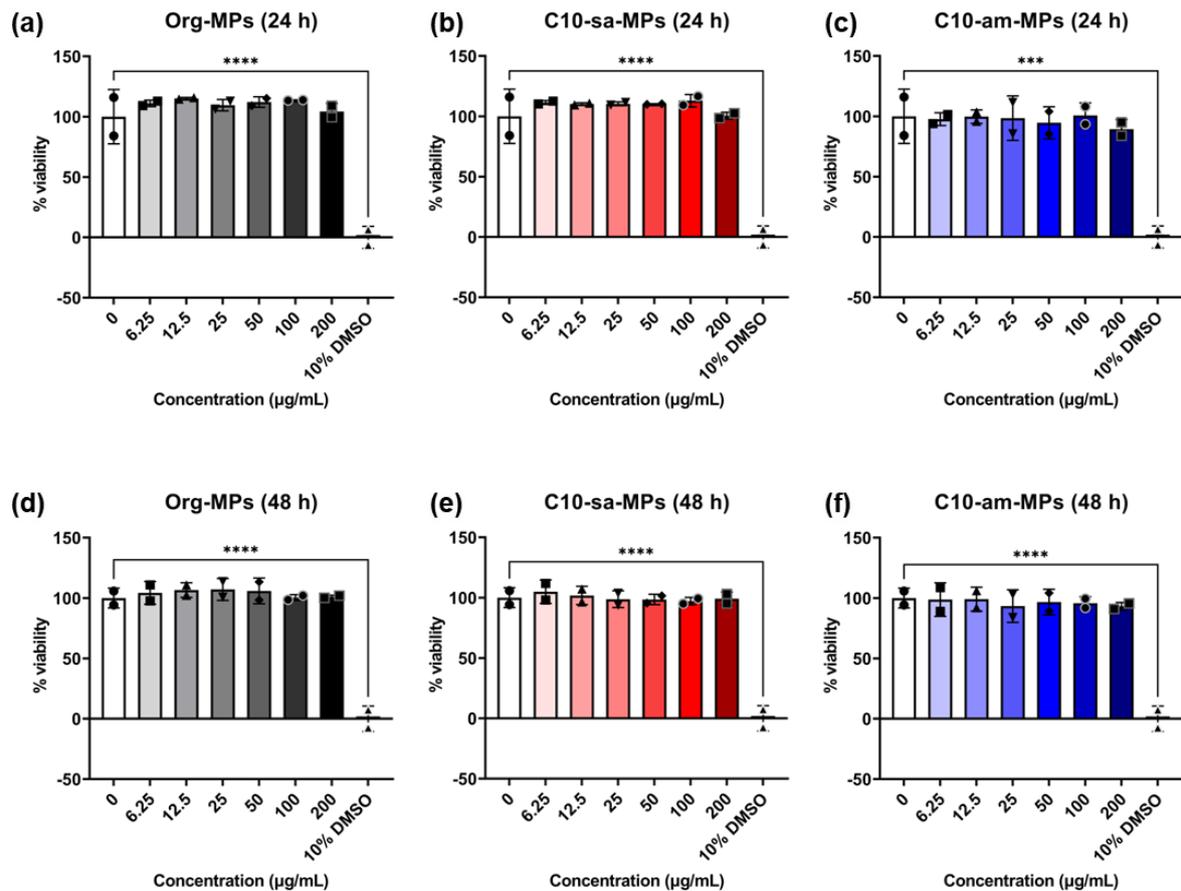


Figure 2: Immunogenicity of Org-, C10-sa-, C10-am-MPs. (a) MP-specific IgM levels (b) MP-specific IgG levels measured by ELISA. 5 mice were used for each treatment group. Ovalbumin (OVA) and mouse serum albumin (MSA) were used as positive and negative control, respectively. The error bars represent the standard deviation of the mean for a sample size of n = 5.

259 **3.3 In vitro cytotoxicity of MPs**

260 The potential cytotoxic effects of MPs were evaluated on Caco-2 cell line to provide valuable insights into its
 261 cytocompatibility. The viability assay utilized 2-(2-methoxy-4-nitrophenyl)-3-(4-nitrophenyl)-5-(2,4-
 262 disulfophenyl)-2H-tetrazolium monosodium salt (WST-8), which is reduced by cellular dehydrogenases to form
 263 a water-soluble, orange-colored product (formazan). The amount of formazan dye produced correlates with the
 264 number of living cells, providing a measure of cell viability [22].

265
 266 According to Figure 3, the cytotoxicity assay against Caco-2 cell lines revealed that all MPs, when compared to
 267 the untreated group, did not exhibit cytotoxicity up to a concentration of 200 µg/mL. This observation suggests
 268 that C10-modification with different linkage type: amide and secondary amine does not compromise the non-
 269 cytotoxic characteristic of hydrophilic ApGln. Furthermore, cell viability was not significantly affected at both
 270 the 24-hour and 48-hour time points, indicating the long-term safety of MPs. Interestingly, tendency of increase
 271 in cell viability was observed upon treatment with Org-MPs and C10-sa-MPs at the 24-hour timepoint; however,
 272 this effect did not extend to the 48-hour mark. This indicates that these MPs treatment show some beneficial effect
 273 on cell viability in the early stages, potentially promoting cell proliferation or enhancing cellular functions [23],
 274 while C10-am-MPs do not possess this effect.



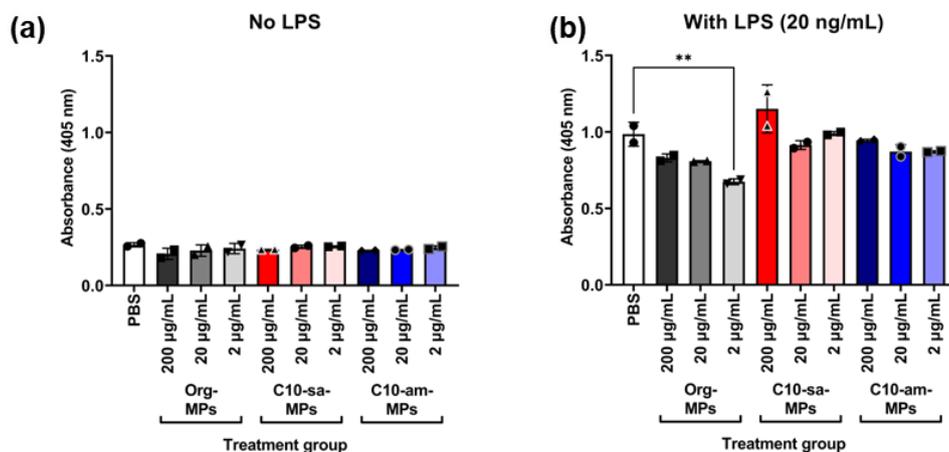
275
 276 Figure 3: Cytotoxicity against Caco-2 cell lines after 24 hours (a-c) and 48 hours (d-f) of exposure to (a, d) Org-
 277 MPs, (b, e) C10-sa-MPs, and (c, f) C10-am-MPs. 10% DMSO were used as positive control. The error bars
 278 represent the standard deviation of two independent experiments, each conducted with a sample size of n = 3.

279 3.4 Anti-inflammatory properties of MPs

280 Immune activation begins when receptors on phagocytes are engaged, initiating signaling cascade. For instance,
 281 lipopolysaccharides (LPS), the major components of outer membrane of Gram-negative bacteria, bind to Toll-like
 282 receptor-4 (TLR-4) on macrophages, initiating an inflammatory response. This binding triggers the activation of
 283 nuclear factor kappa B (NF- κ B) pathway, a crucial mechanism in inflammation [24]. RAW264.7 macrophages
 284 transfected with the SEAP (alkaline phosphatase) reporter gene (SEAP-RAW264.7) were utilized to evaluate NF-
 285 κ B activity. The inflammatory response induced by MPs was evaluated by quantifying secreted alkaline
 286 phosphatase (SEAP) activity, measured based on the hydrolysis of para-nitrophenylphosphate (pNPP) to para-
 287 nitrophenol (pNP), a yellow-colored compound detectable by absorbance.

288
 289 The effect of SEAP secretion upon exposure to varying concentration of each MPs was depicted in Figure 4. In
 290 the absence of LPS, SEAP activity was negligible compared to the control group (PBS). As expected, the addition
 291 of LPS increased SEAP activity, indicating the initiation of an inflammatory response. Treatment of RAW264.7
 292 macrophages with C10-sa-MPs and C10-am-MPs tended to increase SEAP activity compared with Org-MP
 293 treatment. Considering that hydrophobic C10 chains are predominantly localized on the surface [7], these
 294 hydrophobic counterparts may interact more readily with the cell membrane. Consequently, this interaction leads
 295 to an observable trend of increased SEAP activity.

296
 297 In addition, treatment with Org-MPs showed dose-dependent changes in inflammatory responses. At the highest
 298 concentration (200 μ g/mL) of Org-MPs, SEAP activity mirrored that of the control (PBS), but at the lowest
 299 concentration (2 μ g/mL), SEAP activity was significantly decreased. Although a decreasing trend was also
 300 observed in C10-sa-MPs and C10-am-MPs, it was not statistically significant. The decreasing trend suggests that
 301 Org-MPs have the potential to suppress inflammatory responses. However, at higher concentrations, Org-MPs
 302 may induce cellular stress, which could counteract its anti-inflammatory activity. Overall, all three MPs did not
 303 exhibit an additional effect on SEAP activity beyond that induced by LPS alone, suggesting their neutral impact
 304 on LPS-induced inflammation.



305
 306 Figure 4: Anti-inflammatory properties of MPs (a) alone and (b) LPS-induced NF- κ B activation in SEAP-
 307 RAW264.7 macrophages. PBS was used as negative control. The error bars represent the standard deviation of
 308 two independent experiments, each conducted with a sample size of n = 3.

309 **4. Conclusion**

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2 310 In conclusion the non-immunogenic, non-cytotoxic, and anti-inflammatory characteristics of C10-modified MPs
3
4 311 were demonstrated. While C10 modification improves the interfacial strength of MPs under wet conditions in
5
6 312 previous studies, these findings demonstrate that C10-modification with amide or secondary amine linkage
7
8 313 showed similar properties and do not compromise the inherent biocompatibility of ApGln, underscoring their
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10 314 potential safe use in biomedical applications. Further investigation is required to elucidate the underlying
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12 315 mechanisms and to solidify their implications for biomedical applications.
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316 **Statements and Declarations**

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2 317 The authors declare that they have no conflicts of interest relevant to this manuscript.
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5 319 **Data availability**
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8 320 The data presented in this study are available upon request from the corresponding authors.
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19 327 **References**
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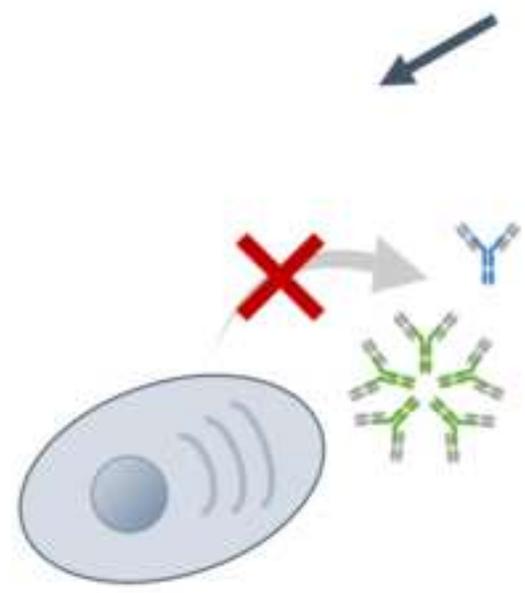
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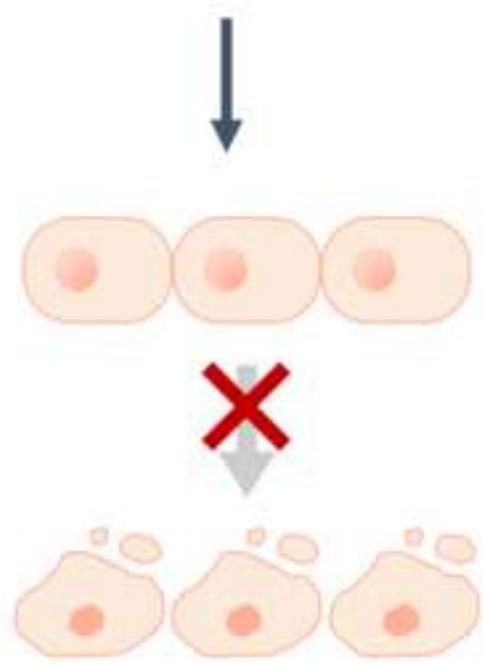
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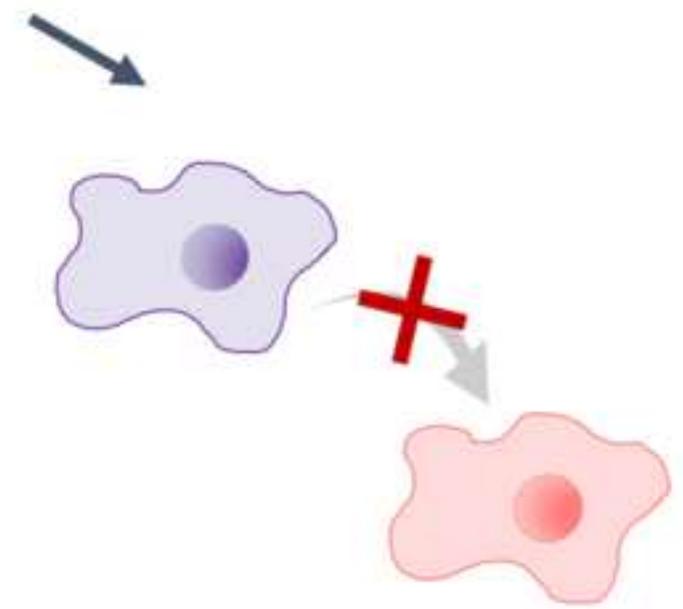
C10-modified Alaska pollock gelatin microparticles



Non-immunogenic



Non-cytotoxic



Non-inflammatory